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## Differential Expression of Genes Involved in the Chronic Response to Intracortical Microelectrodes

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Full length article

## Differential expression of genes involved in the chronic response to intracortical microelectrodes

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### ABSTRACT

Brain-Machine Interface systems (BMIs) are clinically valuable devices that can provide functional restoration for patients with spinal cord injury or improved integration for patients requiring prostheses. Intracortical microelectrodes can record neuronal action potentials at a resolution necessary for precisely controlling BMIs. However, intracortical microelectrodes have a demonstrated history of progressive decline in the recording performance with time, inhibiting their usefulness. One major contributor to decreased performance is the neuroinflammatory response to the implanted microelectrodes. The neuroinflammatory response can lead to neurodegeneration and the formation of a glial scar at the implant site. Historically, histological imaging of relatively few known cellular and protein markers has characterized the neuroinflammatory response to implanted microelectrode arrays. However, neuroinflammation requires many molecular players to coordinate the response - meaning traditional methods could result in an incomplete understanding. Taking advantage of recent advancements in tools to characterize the relative or absolute DNA/RNA expression levels, a few groups have begun to explore gene expression at the microelectrode-tissue interface. We have utilized a custom panel of ~813 neuroinflammatory-specific genes developed with NanoString for bulk tissue analysis at the microelectrode-tissue interface. Our previous studies characterized the acute innate immune response to intracortical microelectrodes. Here we investigated the gene expression at the microelectrode-tissue interface in wild-type (WT) mice chronically implanted with nonfunctioning probes. We found 28 differentially expressed genes at chronic time points (4WK, 8WK, and 16WK), many in the complement and extracellular matrix system. Further, the expression levels were relatively stable over time. Genes identified here represent chronic molecular players at the microelectrode implant sites and potential therapeutic targets for the long-term integration of microelectrodes.

#### Statement of significance

Intracortical microelectrodes can record neuronal action potentials at a resolution necessary for the precise control of Brain-Machine Interface systems (BMIs). However, intracortical microelectrodes have a demonstrated history of progressive declines in the recording performance with time, inhibiting their usefulness. One major contributor to the decline in these devices is the neuroinflammatory response against the implanted microelectrodes. Historically, neuroinflammation to implanted microelectrode arrays has been characterized by histological imaging of relatively few known cellular and protein markers. Few studies have begun to develop a more in-depth understanding of the molecular pathways facilitating device-mediated neuroinflammation. Here, we are among the first to identify genetic pathways that could represent targets to improve the host response to intracortical microelectrodes, and ultimately device performance.

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## 1. Introduction

Intracortical Microelectrode Arrays (MEAs) implanted in the cortex of the brain have been widely used to develop brain-machine interface technologies (BMIs) because of their ability to record high-resolution neural activity [1]. For example, the recorded neural activity can be used to restore lost functions in paralyzed and injured individuals [2–8]. Many basic neuroscience research studies and clinical applications are under consideration and development [9–21]. Unfortunately, implantation of MEAs into the brain breaches the blood-brain barrier, damages brain tissue, and initiates a neuroinflammatory cascade [22–25]. The neuroinflammatory response to MEAs exists if the device remains implanted and significantly contributes to the decline in the quantity and quality of detectable neural activity [14].

Over the last several decades, one primary focus in improving the clinical relevance of BMIs is inhibiting the neuroinflammatory response. Many approaches have been pursued, including (but not limited to): minimizing the trauma associated with device implantation [26,27], minimizing the device/tissue stiffness mismatch [28–36], and reducing oxidative stress/damage [30,37–44]. Inflammatory responses have been broadly targeted either with glucocorticoids such as dexamethasone or anti-inflammatory antibiotics such as Minocycline, or more specifically by altering the quantity or function of specific molecules such as laminin, melatonin, flavopiridol, caspase-1, and CD14 [45–52]. Alternatively, ECM-derived compounds that stimulate neuronal growth have also reduced the inflammatory response against microelectrodes [53,54]. While broadly targeting anti-inflammatory molecules has improved the recording quality in mice [45,46], long-term immune modulation may lead to severe side effects [55–58]. Approaches to reduce microelectrode-induced inflammation should consider that a significant target population of BMI systems is also present with decreased immune function and increased risk for infection [59–62]. Therefore, approaches targeting specific molecules or parts of the inflammatory system may reduce or circumvent some of the side effects of non-specific therapy.

The neuroinflammatory response and subsequent neurodegenerative response are complex. Until recently, the investigation of responsible inflammatory mediators was constrained to only a handful at a time [63]. Utilizing advancements such as developing highly parallel gene expression assays, several groups have begun investigating the expressions of sizable gene sets at the microelectrode-tissue interface [43,64–66]. We started our investigation of gene expression levels associated with the neuroinflammatory response to MEAs focused on a small number of genes concentrated on a specific aspect of the neurodegenerative process – oxidative stress [67]. We then expanded our toolset and characterized the expression of nearly 800 genes at the microelectrode-tissue interface of WT mice at acute time points of up to 2 weeks post-surgery [63,68]. Our initial efforts identified hundreds of differentially expressed genes at acute time points (6H, 24H, 72H, and 2Wks post-surgery). Upregulation of some genes began as early as 6H post-implantation, while others started between 72H to 2Wks post-surgery. As an example, the cluster of differentiation 14 (*Cd14*) gene, a molecule in the Pathogen Recognition Receptor (PRR) pathway, was upregulated in response to microelectrode implantation at several time points post-surgery [63]. In corroboration of these findings, it is essential to recall that *Cd14*<sup>-/-</sup> mice exhibited improved microelectrode recording quality at acute time points [47]. Further, we found differential gene expression for cytokine, chemokine, and complement pathways at acute time points to be similar in *Cd14*<sup>-/-</sup> and WT. However, the time to peak expression level was delayed in *Cd14*<sup>-/-</sup> mice compared to WT mice (72 hours in *Cd14*<sup>-/-</sup> mice vs. 24 hours in WT mice) [68]. Thus, based on our studies as well as that of other labs, cy-

tokine, chemokine, and complement pathways have been identified as central pathways in the neuroinflammatory response against microelectrodes, with many members differentially expressed at acute time points post-surgery [43,63–65,68].

Recently, the Purcell and Hofmann groups have begun to explore the transcriptomic analysis of the microelectrode interface [65,66]. Some technologies, such as 10x genomics, allow for in-depth coverage of gene expression with spatial resolution – representing great promise for improving our understanding of the microelectrode-tissue interface. However, such techniques can quickly become cost-prohibitive and more challenging to scale up for larger sample sets. Therefore, we have again utilized a custom gene set of ~800 neuroinflammatory-specific genes developed with NanoString for bulk analysis of the tissue adjacent to the microelectrode-tissue interface. Many of the molecular players identified in previous acute-time point focused studies are early responders that show decreased upregulation by 2WK post-surgery, with most genes showing peak upregulation 24 – 72 hours post-surgery. Therefore, we hypothesized that the profile of molecular players at chronic time points post-surgery would differentiate from that of acute time points. Here, we expected fewer upregulated genes in the neuroinflammatory pathway, with later-stage upregulation of anti-inflammatory and wound-healing molecules. Here, we will report our findings for WT mice implanted with MEAs for 4WK, 8WK, and 16WK post-surgery.

## 2. Materials and methods

The materials and methods used in this paper were previously described. Refer to Bedell et al. [63] and Song et al. [68] for more details. Briefly:

### 2.1. Animals

We performed all animal care, handling, and procedures in compliance with a protocol approved by the Institutional Animal Care and Use Committee (IACUC) at Case Western Reserve University. Twenty male C57BL/6J mice (Jackson Laboratory Strain #003724) were obtained from Jackson laboratory between 7 – 10 weeks of age and housed for 1 – 4 weeks before surgery was performed in a class II sterile hood using microisolator techniques. Mice were housed at 3–5 per cage before surgery and 1 per cage post-surgery to prevent physical damage to the microelectrodes or implant sites. The surgeon was blinded from the survival duration group (4WK, 8WK, or 16WK). An additional set of control mice (non-surgical control mice) did not receive any surgical procedures. The 20 mice were divided equally among the three experimental and one control group for an N = 5 per group.

### 2.2. Nonfunctional “dummy” microelectrode probes

Nonfunctional “dummy” silicon probes were received from the Pancrazio and Cogan Laboratories at the University of Texas at Dallas [69,70]. Dummy probes mirrored the physical dimensions of single-shank Michigan-style microelectrode arrays. Probes were 15 μm thick, 123 μm wide along the widest parts of the shank, and 2 mm long from base to tip. Before implantation, dummy probes were washed by soaking in 95% ethanol solution three times for 5 minutes each and sterilized by cold ethylene oxide gas following established protocols [71–73].

### 2.3. Surgical procedure

Before surgery, each mouse was anesthetized with isoflurane (3% in 1.0 L/min O<sub>2</sub> for induction, 2% in 1.0 L/min O<sub>2</sub> for main-

tenance) and placed in a stereotactic frame. Once anesthetized, Meloxicam (2 mg/kg) and Buprenorphine (0.05 mg/kg) were given subcutaneously as a systemic analgesic. While Meloxicam can inhibit neuroinflammation, the effects are short-lived, with a half-life of ~20 hours, and is thus not expected to impact the chronic neuroinflammatory response studied here [74]. The surgical site was prepared by first shaving the hair, then treated with local analgesic (0.2 ml of 0.25% Marcaine subcutaneously), and sterilized with alternating betadine and isopropanol swabs. A ~1 cm midline incision exposed the skull. Then, we cleaned the tissue adhered to the skull with a hydrogen peroxide swab. Four craniotomies were drilled following established protocols to minimize damage to the blood-brain barrier [26,75], using a 0.45 mm dental drill bit: 1.5 mm lateral and 1.0 mm anterior and posterior to the bregma. Nonfunctional dummy probes were manually inserted into each hole to approximately 1.0–1.5 mm in depth at the speed of ~ 2 – 3 mm/s. Kwik-Sil was used to seal the craniotomies, and dental cement (Flow-It) tethered the dummy probes to the skull. The skin was closed with a 5-0 monofilament polypropylene suture. Meloxicam (2 mg/kg, SQ) and Buprenorphine (0.05 mg/kg, SQ) were administered for three days post-operatively for pain management. Pre-surgical naïve sham mice were used as controls (Non-Surgical Control, or NSCTR) for later comparison.

#### 2.4. Tissue extraction

Mice were anesthetized with a ketamine-xylazine cocktail (100mg/Kg and 10mg/Kg, respectively) to a deep surgical plane for euthanasia via cardiac perfusions with cold 1X phosphate-buffered saline (PBS). Perfusions required 50–100 mL PBS for the exudate to run clear. To prevent excessive RNA degradation, we immediately extracted mouse brains. Probes were explanted before flash freezing of the brains in optimal cutting temperature compound (OCT). We stored frozen brains at -80°C until further processing. Cortical brain tissues surrounding the neural probes were cryo-sectioned into 150 µm thick frozen slices. We collected six to seven 150 µm thick sections for this study and stored eight to ten 5 µm thick sections randomly distributed between thicker sections for future studies.

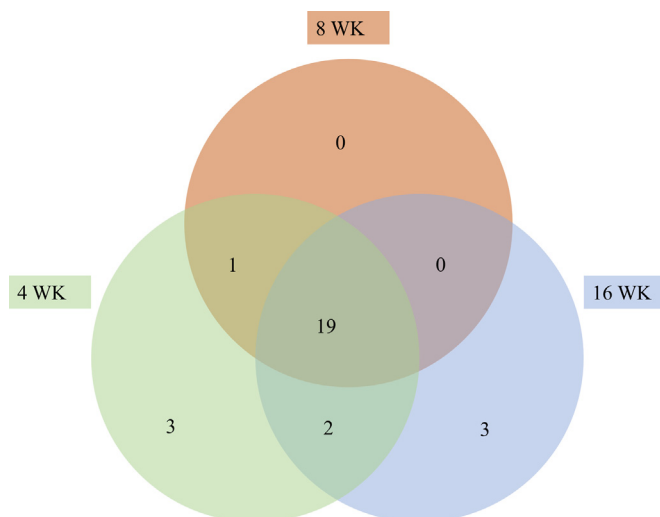
#### 2.5. RNA isolation

Extracted brain tissue was homogenized by placing collected samples directly into 2.0 mL homogenization microtubes prefilled with 1.5 mm zirconium beads (Benchmark scientific D1032-15) and 1 mL Qiazol (RNA extraction lysate) [63]. The microtubes were then loaded onto a Bead Bug Homogenizer (Benchmark Scientific D1030) and shaken at 4000 rpm for 1 min.

The RNA was extracted and purified from the homogenized tissue using RNeasy® Plus Universal Mini Kit (Qiagen 73404) at the Gene Expression and Genotyping Facility at Case Western Reserve University. RNA quality and quantity were determined using Nanodrop. We concentrated samples with low concentration with a Speedvac. Isolated RNA was stored at -80°C for up to two months before sequencing.

#### 2.6. Gene expression assay

We used a barcode technology developed by NanoString Technologies (Seattle, WA) to determine gene expression by counting individual genes. We hybridized RNA (~100 ng per sample) with a codeset containing capture probes and reporter probes genes of interest. Here, we utilized a codeset containing 826 genes; 758 were target genes from the nCounter® Mouse Neuroinflammation Panel, with 13 additional housekeeping genes and 55 cus-



**Fig. 1.** Gene expression at the microelectrode-tissue interface. Venn Diagram indicating the number of genes differentially expressed for each time point examined, compared to the NSCTR mice at chronic time points. Overlapping regions of the Venn diagrams were used to show an overlap of differentially expressed genes at 4WK, 8WK, and 16WK post-surgery compared to naïve sham control mice,  $P_{adj} < 0.05$  and  $\text{Log}_2\text{FoldChange} > 1$  or  $< -1$ .

tom genes of interest (Table 1). Negative controls and positive controls were spiked in. Samples were incubated at 65°C for 16 hours, loaded onto cartridges, and processed with nCounter® Max Analyzer. Measurements were taken at 280 Field-of-View per sample, and the relative number of each gene was determined from absolute counts of fluorescent barcode reporters using the nCounter® MAX Analyzer.

#### 2.7. Statistical analysis

##### 2.7.1. Normalization

Normalization was performed following established protocols utilizing nSolver, provided by NanoString Technologies [68]. Each sample's raw counts were normalized to raw spiked-in positive controls and housekeeping gene controls. In this study, we utilized ten housekeeping genes for normalization (Table 1), while genes with counts below 25 in 85% of the samples were excluded from the analysis. Here, 242 genes were removed from analysis based on the exclusion criteria leaving 571 genes for further analysis (Fig. 1).

##### 2.7.2. Comparison of gene expression at each post-surgical time point to naïve non-surgical control

As previously described, changes in gene expression were presented as a ratio between each time point (4WK, 8WK, and 16WK) to the single group of pre-surgical naïve sham mice (non-surgical control mice or NSCTR) [68] in a pairwise fashion. Bilateral implantation of the mice prevented contralateral tissue from being used as a non-surgical control. The ratio was then plotted on a  $\text{Log}_2$  scale (henceforth called  $\text{Log}_2\text{FoldChange}$ ). The standard error of the mean was calculated and plotted for each pair. An unpaired T-test with Benjamini-Yekutieli False-Discovery-Rate Correction is used to determine statistical significance. Significance is set at p-value adjusted ( $P_{adj}$ )  $< 0.05$ .

Genes with altered expression at threshold  $\text{Log}_2\text{FoldChange} > 1$  or  $< -1$  (i.e., 2-fold increase or decrease in expression),  $P_{adj} < 0.05$ , at overlapping time points, were counted and visualized with a Venn diagram. Volcano plot and pathway analysis are generated using the Advanced Analysis Plug-in of nSolver. Bar graphs of altered expression of specific genes are generated using Matlab.



**Table 2**

Gene expression at the microelectrode-tissue interface. Differentially expressed genes at 4WK, 8WK, and 16WK post-surgery are listed. Genes with differential expression of  $P_{adj} < 0.05$  and  $Log_2FoldChange > 2$  or  $< -2$  are in green; genes with differential expression of  $P_{adj} < 0.05$  and  $Log_2FoldChange$  between 1 – 2 and -1 to -2 are in blue. The molecular pathway these genes fall under is listed in Table 3.

4WK				8WK				16WK			
Gene	Log2 Fold Change	std error (log2)	Padj	Gene	Log2 Fold Change	std error (log2)	Padj	Gene	Log2 Fold Change	std error (log2)	Padj
								<i>Anxa1</i>	1.42	0.417	0.0199
<i>Arc</i>	-1.14	0.305	0.0106								
<i>Bcl2a1a</i>	1.64	0.272	2.78E-05	<i>Bcl2a1a</i>	1.25	0.275	0.0018	<i>Bcl2a1a</i>	1.56	0.273	7.39E-05
								<i>Blnk</i>	1.13	0.224	0.0004
<i>C3</i>	2.64	0.554	0.0008	<i>C3</i>	2.48	0.556	0.0019	<i>C3</i>	3.53	0.546	8.77E-06
<i>C3ar1</i>	1.22	0.302	0.0050								
<i>C4a</i>	3.01	0.335	1.84E-08	<i>C4a</i>	3.08	0.335	1.54E-08	<i>C4a</i>	3.48	0.334	1.15E-09
<i>Cd36</i>	2.66	0.641	0.0042	<i>Cd36</i>	2.86	0.64	0.0019	<i>Cd36</i>	2.76	0.64	0.0027
<i>Cd68</i>	1.45	0.237	2.65E-05	<i>Cd68</i>	1.20	0.238	0.0005	<i>Cd68</i>	1.31	0.237	0.0001
<i>Cd74</i>	1.93	0.478	0.0050	<i>Cd74</i>	2.00	0.477	0.0037	<i>Cd74</i>	1.78	0.478	0.0106
<i>Cd84</i>	1.47	0.247	3.41E-05	<i>Cd84</i>	1.38	0.248	0.0001	<i>Cd84</i>	1.49	0.247	3.02E-05
<i>Clec7a</i>	3.20	0.47	3.74E-06	<i>Clec7a</i>	2.81	0.474	5.50E-05	<i>Clec7a</i>	3.15	0.47	4.81E-06
<i>Ctss</i>	1.34	0.177	6.35E-07	<i>Ctss</i>	1.20	0.177	6.96E-06	<i>Ctss</i>	1.26	0.177	2.32E-06
<i>Fcer1g</i>	1.20	0.218	0.0001					<i>Fcer1g</i>	1.03	0.219	0.0010
<i>Fcgr2b</i>	1.66	0.253	6.89E-06	<i>Fcgr2b</i>	1.52	0.253	5.34E-05	<i>Fcgr2b</i>	1.71	0.253	4.25E-06
<i>Gfap</i>	2.45	0.355	3.56E-06	<i>Gfap</i>	2.12	0.355	5.34E-05	<i>Gfap</i>	2.41	0.355	4.25E-06
								<i>H2-T23</i>	1.22	0.217	9.46E-05
<i>Lcn2</i>	1.89	0.494	0.0084					<i>Lcn2</i>	1.84	0.494	0.0106
<i>Lilrb4a</i>	2.85	0.472	2.78E-05	<i>Lilrb4a</i>	2.53	0.474	0.0003	<i>Lilrb4a</i>	2.50	0.474	0.0002
<i>Mpeg1</i>	1.56	0.211	9.94E-07	<i>Mpeg1</i>	1.30	0.212	4.24E-05	<i>Mpeg1</i>	1.50	0.211	2.32E-06
<i>Mmp12</i>	5.41	0.561	4.75E-09	<i>Mmp12</i>	5.39	0.561	1.03E-08	<i>Mmp12</i>	5.66	0.561	1.41E-09
<i>Psmb8</i>	1.04	0.265	0.0070	<i>Psmb8</i>	1.27	0.263	0.0009	<i>Psmb8</i>	1.16	0.264	0.0022
<i>Ptx3</i>	1.87	0.431	0.0024								
<i>Serpina3n</i>	2.53	0.251	2.84E-09	<i>Serpina3n</i>	2.20	0.253	4.23E-08	<i>Serpina3n</i>	2.41	0.251	3.43E-09
<i>Spp1</i>	3.46	0.398	3.32E-08	<i>Spp1</i>	3.31	0.398	9.93E-08	<i>Spp1</i>	3.78	0.398	3.43E-09
<i>Tnfrsf25</i>	-1.36	0.276	0.0006	<i>Tnfrsf25</i>	-1.22	0.275	0.0019				
<i>Tyrobp</i>	1.22	0.208	3.68E-05	<i>Tyrobp</i>	1.07	0.208	0.0004	<i>Tyrobp</i>	1.14	0.208	0.0001
<i>Vim</i>	1.71	0.25	3.74E-06	<i>Vim</i>	1.44	0.251	8.85E-05	<i>Vim</i>	1.73	0.25	3.36E-06

Overall gene expression is stable between 4WK to 16WK post-surgery: expression change skews towards upregulation, with more genes showing upregulation than downregulation. Most genes show differential expression below statistical significance ( $P_{adj} > 0.05$ ), and of those genes showing upregulation above statistical significance, most show a  $Log_2FoldChange > 1$  or  $< -1$  (which corresponds to linear fold change  $> 2$  or  $< -2$ ).

Genes with differential expression at 4WK, 8WK, and 16WK post-surgery compared to NSCTR above the threshold of  $Log_2FoldChange > 1$  or  $< -1$  are listed in Table 2. Additionally, genes with differential expression above a higher threshold of  $Log_2FoldChange > 2$  or  $< -2$  are labeled in green, which are: *C3*, *C4a*, *Cd36*, *Clec7a*, *Gfap*, *Lilrb4a*, *Mmp12*, *Serpina3n*, and *Spp1*. These nine genes, which show the highest upregulation at 4–16WK post-surgery, show upregulation above the threshold of  $Log_2FoldChange > 2$  or  $< -2$  at all post-surgical time points in this study. *Mmp12* is the highest expressed gene at all time points examined in this study, with  $Log_2FoldChange$  between 5.39 – 5.99.

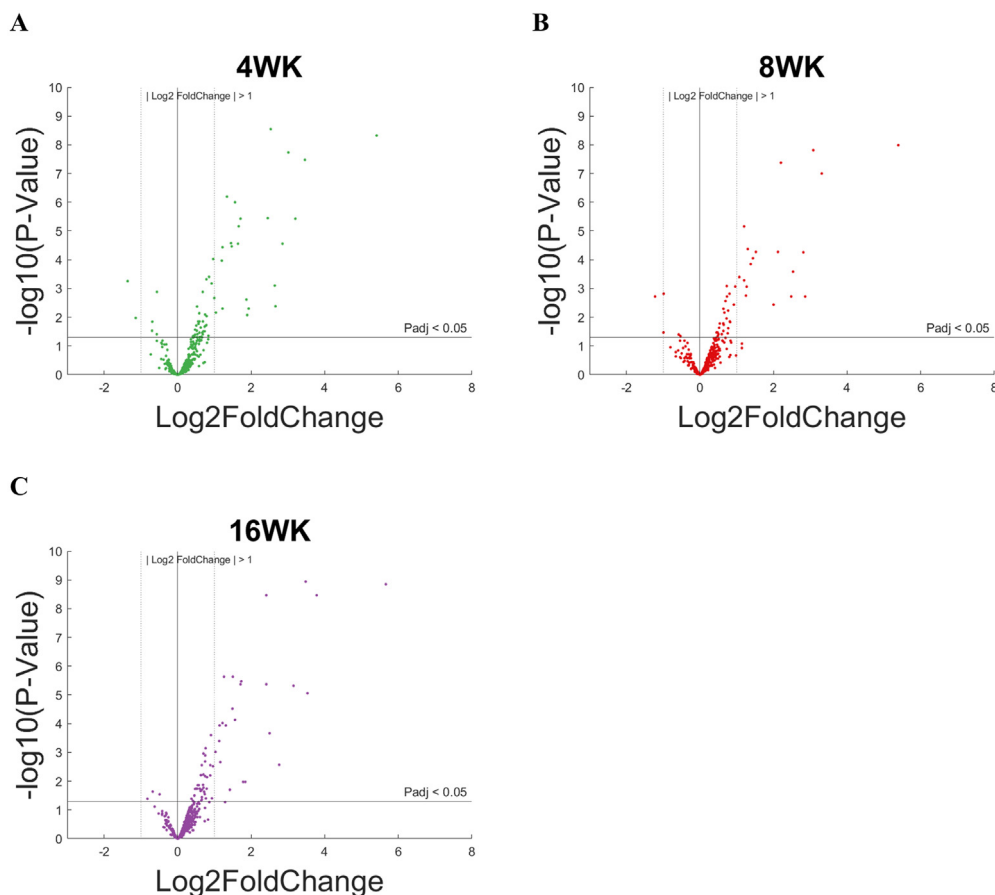
The pathways associated with the differentially expressed genes in Table 2 are listed in Table 3. These differentially expressed genes identified in this study are enriched for proteins involved in neutrophil degranulation, complement system, cell surface receptors (pattern recognition receptors and others), extracellular matrix, and adaptive immune system. Some genes fall into several categories.

#### 4. Specific gene differential expressions

##### 4.1. Complement system

The complement system is part of the innate immune system and consists of circulating proteins, cell surface regulators, and effectors. The complement system is activated by invading pathogens and tissue damage via classical, lectin-binding, and alternative pathways, converging at the amplification step of C3 [76]. The protein C3 is a critical molecule in the amplification step of the complement activation cascade, and the protein C4a is a subunit of C4 and a by-product of C4 activation. C4 is also involved in the amplification step of the complement activation cascade.

Fig. 3 a (and Table 2) compares the gene complement 3 (C3) between each post-surgical time point evaluated in the study. At 4WK and 8WK post-surgery, C3 expression displayed 2.64X and 2.48X  $Log_2FoldChange$  compared to NSCTR. At 16WK post-surgery, C3 expression increased to 3.53X  $Log_2FoldChange$  compared to NSCTR. However, a comparison between 8WK or 16WK post-surgery to 4WK post-surgery and between 8WK and 16WK post-surgery showed no statistically significant differential expression between each pair. The gene complement 4 subunit a (*C4a*) demonstrated a similar trend (Fig. 3b, Table 2), showing 3.01X and 3.08X  $Log_2FoldChange$  compared to NSCTR at 4WK and 8WK post-surgery, and slightly increased to 3.48X  $Log_2FoldChange$  at 16WK



**Fig. 2.** Volcano plots of genes with differential expression at (a) 4WK, (b) 8WK, and (c) 16WK compared to NSCTR. Genes with differential expression of  $\text{Log}_2\text{FoldChange} > 1$  or  $< -1$  and  $P_{\text{adj}} < 0.05$  are labeled.

post-surgery. Genes encoding for both the receptor for C3 subunit a (*C3ar1*) and pentraxin-3 (*Ptx3*) showed a significant (1.22X and 1.87X, respectively)  $\text{Log}_2\text{FoldChange}$  compared to NSCTR at 4WK post-surgery (Fig. 3c-d, Table 2). Note that for *C3ar1* expression at 16WK,  $\text{Log}_2\text{FoldChange} < 1$  (0.848) compared to NSCTR, below the threshold of  $\text{Log}_2\text{FoldChange} > 1$  or  $< -1$ ; therefore, *C3ar1* did not meet the criteria for differential expression at 16WK post-surgery. Like the trend displayed for C3, for *C4a*, *C3ar1*, and *Ptx3*, pairwise comparison between 4WK, 8WK, and 16WK post-surgery showed no statistically significant differential expression between any of these pairs – indicating no changes in expression over 4WK to 16WK post-surgery.

#### 4.2. Extracellular matrix

The extracellular matrix forms a scaffold around the cells in the brain and maintains tissue integrity and communication between cells [77]. During injury and inflammation of brain tissue, such as following the implantation of microelectrodes, the extracellular matrix is actively remodeled as part of the wound healing process [78,79].

Fig. 4 and Table 2 highlights the genes examined in our set that encode proteins associated with the extracellular matrix and displayed significance indicated by  $P_{\text{adj}} < 0.05$ . In Fig. 4a (Table 2). Our results demonstrate that the expression of genes encoding for Matrix Metalloproteinase 12 (*Mmp12*) show a 5.41X, 5.39X, and 5.66X  $\text{Log}_2\text{FoldChange}$  compared to NSCTR at 4WK, 8WK, and 16WK post-surgery, respectively. The expression of *Mmp12* was detected as stable throughout the study; pairwise comparison between 4WK, 8WK, and 16WK showed no significant difference in

expression levels between any of the three examined time points. Genes encoding for Secreted Phosphoprotein 1 (*Spp1*, Fig. 4b and Table 2) also showed a stable upregulation over the course of this study: 3.46X, 3.31X, and 3.78X  $\text{Log}_2\text{FoldChange}$  at 4WK, 8WK, and 16WK post-surgery, respectively. Genes encoding for Cathepsin S (*Ctss*, Fig. 4c and Table 2) show a stable upregulation of 1.34X, 1.20X, 1.26X  $\text{Log}_2\text{FoldChange}$  compared to NSCTR at 4WK, 8WK, and 16WK post-surgery, respectively. As with *Mmp12* and *Spp1*, *Ctss* expression was statistically unchanged from 4WK to 16WK post-surgery. All three genes associated with the extracellular matrix that demonstrated a significant change in expression level ( $P_{\text{adj}} < 0.05$  for comparisons between the time point and NSCTR) displayed consistent expression levels, regardless of the duration post-implantation.

#### 4.3. Cellular receptors

Cellular responses to the environment, or environmental changes, are primarily facilitated through receptor-ligand interactions. In this section, we group several classes of cellular receptors involved in the neuroinflammatory response. Here, cell receptors associated with the pattern recognition receptor (PRR) family (*Cd36*, *Clec7a*), receptors for immunoglobulins (*Fcgr1g*, *Fcgr2b*), as well as leukocyte-associated immunoglobulin-like receptors (*Lilrb4a*) are discussed due to their significant changes following microelectrode implantation (Fig. 5 and Table 2).

Fig. 5a and Table 2 demonstrates that expression of Cluster of Differentiation 36 (*Cd36*) showed a steady  $\text{Log}_2\text{FoldChange}$  of 2.66X, 2.86X, 2.76X compared to NSCTR at 4WK, 8WK, and 16WK post-surgery. A pairwise comparison between 4WK, 8WK, and

**Table 3**

The molecular pathways of differentially expressed genes at 4WK, 8WK, or 16WK post-surgery (threshold at Log2FoldChange > 1 or < -1, P<sub>adj</sub> < 0.05). The Log2FoldChange, Std Error in log<sub>2</sub> and P<sub>adj</sub> of these genes are listed in Table 2.

Genes	Full name of Genes	Neutrophil Degranulation	Complement System	PRR/ IgR	Extracellular Matrix	Adaptive Immune System	Others
<i>Anxa1</i>	Annexin A1						Intracellular Signaling
<i>Arc</i>	Activity Regulated Cytoskeleton Associated Protein						Intracellular Signaling
<i>Bcl2a1a</i>	BCL2 Related Protein A1						apoptosis
<i>Blnk</i>	B-cell linker					yes	Intracellular Signaling
<i>C3</i>	Complement C3	yes	yes			yes	Intracellular Signaling, Metabolism
<i>C3ar1</i>	Complement C3a Receptor 1	yes	yes				Intracellular Signaling
<i>C4a</i>	Complement C4A		yes				
<i>Cd36</i>	Cluster of Differentiation 36	yes		yes		yes	metabolism, Vesicle-mediated transport
<i>Cd68</i>	Cluster of Differentiation 68						Cell Adhesion
<i>Cd74</i>	Cluster of Differentiation 74					yes	
<i>Cd84</i>	Cluster of Differentiation 84						
<i>Clec7a</i>	C-Type Lectin Domain Family 7 Member A			yes			
<i>Ctss</i>	Cathepsin S	yes		yes	yes	yes	
<i>Fcεr1g</i>	Fc Epsilon Receptor 1g	yes		yes			
<i>Fcγr2b</i>	Fc Gamma Receptor 2b	yes		yes		yes	
<i>Gfap</i>	Glial Fibrillary Acidic Protein						Cytoskeleton
<i>H2-T23</i>	H2-T23	yes				yes	
<i>Lcn2</i>	Lipocalin 2	yes					Transport of small molecules
<i>Lilrb4a</i>	Leukocyte Immunoglobulin Like Receptor B4	yes					
<i>Mmp12</i>	Matrix Metalloprotease 12				yes		
<i>Mpeg1</i>	Macrophage Expressed 1						Anti-microbial
<i>Psmβ8</i>	Proteasome 20S Subunit Beta 8					yes	Cytokine, cell cycle, transcription
<i>Ptx3</i>	Pentraxin	yes	yes				
<i>Serpina3n</i>	Serpin Family A Member 3						protease
<i>Spp1</i>	Secreted Phosphoprotein 1				yes		Intracellular Signaling, Metabolism
<i>Tnfrsf25</i>	TNF Receptor Superfamily Member25						Cytokine Receptor, Intracellular Signaling
<i>Tyrbp</i>	Transmembrane Immune Signaling Adaptor TYROBP	yes					Developmental Biology
<i>Vim</i>	vimentin						cytoskeleton

16WK showed that *Cd36* expression levels were not significantly different.

Fig. 5b and Table 2 demonstrated that genes encoding for C-Type Lectin Domain Family 7 Member A (*Clec7a*) showed an upregulation of 3.20X, 2.81X, 3.15X Log2FoldChange at 4WK, 8WK, and 16WK post-surgery, respectively. Expression levels were highest at 4WK and 16WK post-surgery. However, pairwise comparison showed that expression levels at 8WK post-surgery were not significantly different from those at 4WK or 16WK. Genes encoding for Leukocyte Immunoglobulin Like Receptor B4 (*Lilrb4a*) showed an upregulation in Log2FoldChange of 2.85X, 2.53X, and 2.50X at 4WK, 8WK, and 16WK post-surgery, respectively (Fig. 5c and Table 2). Pairwise comparison showed that expression levels at 4WK post-surgery were not significantly different from those at 8WK or 16WK.

Genes encoding for IgE receptor Fc E Receptor 1g (*Fcεr1g*, Fig. 5d and Table 2) and IgG receptor Fc G Receptor 2b (*Fcγr2b*, Fig. 5e and Table 2) showed a small yet consistent upregulation at 4WK to 16WK post-surgery. *Fcεr1g* showed Log2FoldChange of 1.2X and 1.03X at 4WK and 16WK post-surgery. Note that at 8WK post-surgery, the Log2FoldChange < 1 (0.921) compared to NSCTR; therefore, *Fcεr1g* did not meet our criteria as differentially expressed at 8WK post-surgery. *Fcγr2b* showed 1.66X, 1.52X, and 1.71X Log2FoldChange compared to NSCTR at 4WK, 8WK, and 16WK post-surgery, respectively. While the expression level of *Fcγr2b* decreased slightly from 4WK to 8WK, only to increase again at 16WK, each time point showed significantly higher *Fcγr2b* ex-

pression than NSCTR, and pairwise comparison indicated that the expression at each time point was not statistically different from each other.

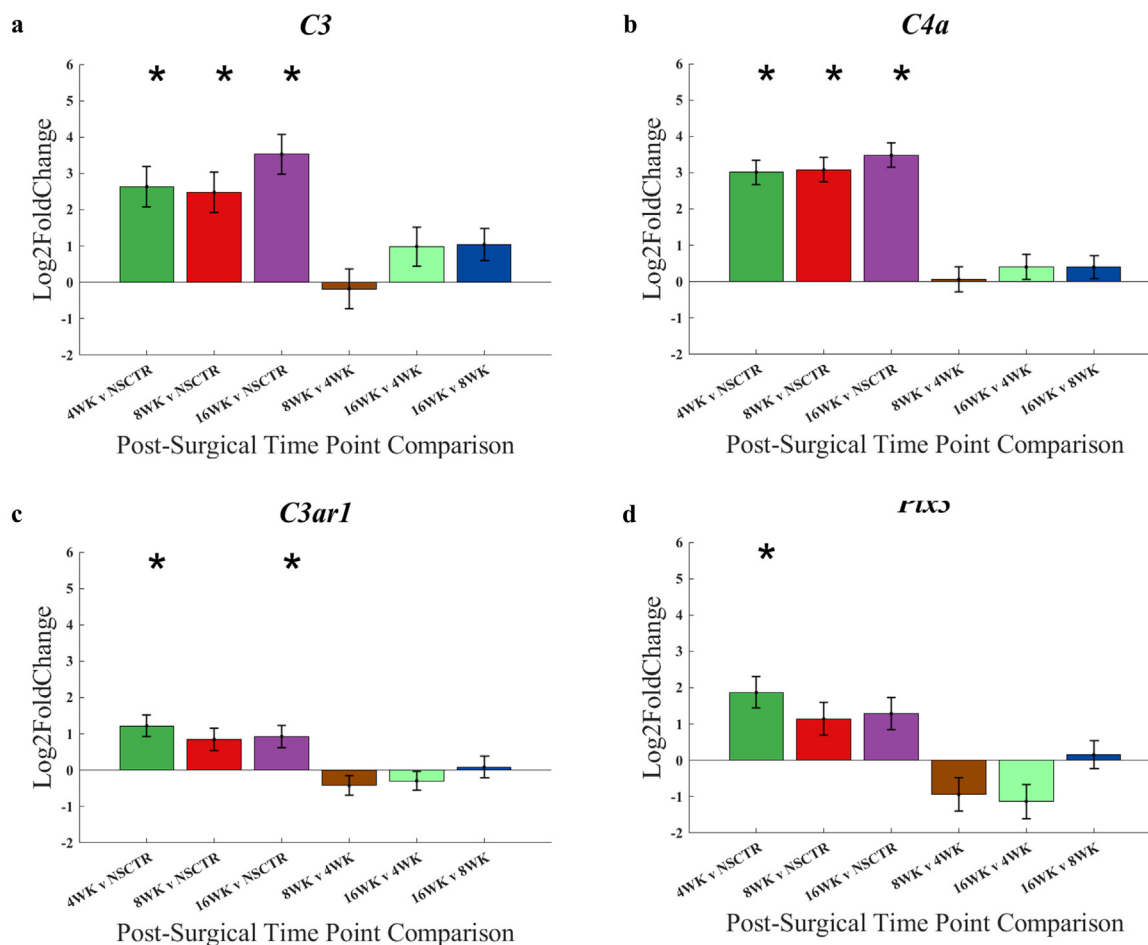
#### 4.4. Other highly differentially expressed genes

Genes encoding for *Gfap* displayed a consistently elevated expression level of 2.45X, 2.12X, and 2.41X Log2FoldChange at 4WK, 8WK, and 16WK post-surgery. Further, there were no significant differences in the expression levels between each time point pair (Fig. 6a, Table 2). Genes encoding for Serine peptidase inhibitor clade A member 3n (*Serpina3n*) showed a Log2FoldChange of 2.53X, 2.20X, and 2.41X at 4WK, 8WK, and 16WK post-surgery compared to NSCTR. No statistically significant differences were detected between any time point pairs, indicating that *Serpina3n* gene expression was stably upregulated throughout this study (Fig. 6b, Table 2).

#### 4.5. Considering gene expression acute time points

To better chronicle the differential expression of genes over time, data from a previous study that used the same methodology used here but for acute time points of 6H, 24H, 72H, and 2WK post-surgery [63] were included in the current chronic data set. The present study used an expanded panel of 826 genes compared to the 791 in the original study. The pre-surgical, naïve sham





**Fig. 3.** Bar graphs presenting the differential gene expression of (a) *C3*, (b) *C4a*, (c) *C3ar1*, and (d) *Pt3* at 4WK vs. NSCTR (green), 8WK (red) vs. NSCTR, and 16WK vs. NSCTR (purple), 4WK vs. 8WK (brown), 4WK vs. 16WK (lime green), and 8WK vs. 16 WK (navy blue). The height of each bar illustrates the Log2FoldChange of the comparison. The error bar indicates the standard error of the mean between gene expressions at each time point. Asterisk (\*) denotes  $P_{adj} < 0.05$ .

control used in the previous study (NSCTR) discussed in this section is a different set of animals from those used in the current study.

Of the 791 genes investigated in the previous study, 13 are housekeeping genes used for normalization. Of the remaining 778 genes, 189 were removed from analysis based on the exclusion criteria, leaving 589 genes to be discussed. Of the 589 genes, 61 showed no differential expression at any time point in the study (not represented below). In total, 536 genes showed differential expression at 6H, 24H, 72H, or 2WK post-surgery. The Venn diagram (Fig. 7) indicates the number of genes differentially expressed at each time point in the previous study.

Overall, there are 65 genes showing differentially expressed throughout 6H to 2WK post-surgery. At 6H post-surgery, a total of 153 genes showed differential expression. One gene showed differential expression at only 6H post-surgery. At 24H post-surgery, 501 genes showed differential expression, including 151 genes exhibiting differential expression at 6H post-surgery and 350 newly differentially expressed genes. Eighty-nine genes showed differential expression at only 24H post-surgery. At 72H post-surgery, 181 genes showed differential expression, including 175 that showed differential expression at 24H post-surgery and six newly differentially expressed genes. One gene showed differential expression at only 72H post-surgery. No genes showed differential expression at 6H and 72H but not 24H post-surgery. At 2WK, 358 genes showed differential expression, with 139 maintaining differential expression from 72H. One hundred sixty-five genes showed differential ex-

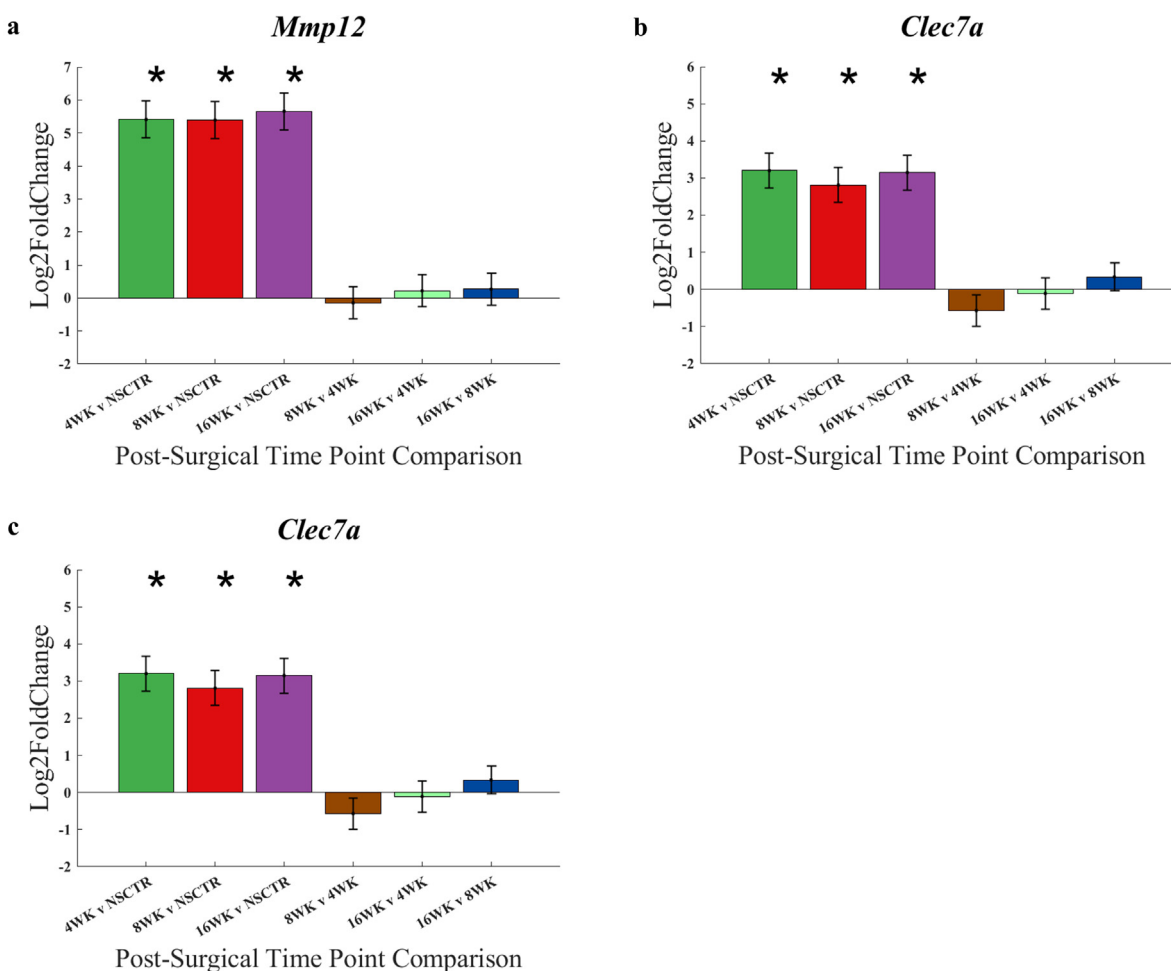
pression at only 24H and 2WK, 34 showed differential expression at 6H, 24H, and 2WK, and one gene showed differential expression at 6H and 2WK. Nineteen genes showed differential expression at 2WK only.

## 5. Discussion

Overall, by chronic time points (4WK to 16WK), fewer genes show differential expression compared to acute time points (6H to 2WK), and the gene expression becomes more stable. Most of the 28 genes exhibiting differential expression at 4WK to 16WK are in the complement, extracellular, or cell receptor pathways. Nineteen of these genes show overexpression at 4WK, 8WK, and 16WK post-surgery and exhibit a similar expression level at these time points. Therefore, at 4WK to 16WK post-surgery, the ongoing neuroinflammation and neurodegeneration are driven stably by a specific set of complement, extracellular, or cell receptor pathways.

### 5.1. Complement system

In previous studies, we have found that many members of the complement system displayed high upregulation at acute time points (6H to 2WK) post-surgery, with *C3* showing increasing upregulation over the course of 6H to 2WK post-surgery [63,68]. Many labs have identified *C3* as an essential player in neuroinflammatory response to intracortical microelectrode implantation and suggested that inhibition of *C3* could result in a potential ther-



**Fig. 4.** Bar graph of differential gene expression of (a) *Mmp12*, (b) *Spp1*, and (c) *Ctss* at 4WK vs. NSCTR (green), 8WK vs. NSCTR (red), and 16WK vs. NSCTR (purple), 4WK vs. 8WK (brown), 4WK vs. 16WK (lime green), and 8WK vs. 16WK (navy blue). The height of each bar shows the Log2FoldChange of the comparison. The error bar indicates the standard error of the mean between gene expressions at each time point compared. Asterisk (\*) denotes  $P_{adj} < 0.05$  for the time point and NSCTR comparisons.

apeutic target [63–65,68]. *C4a* codes for a subunit of C4 and a marker of C4 activation; C4 activation is upstream of C3 activation [80]. *C3ar1* codes for the cellular receptor of C3a, a subunit of C3 and a marker of C3 activation [80]. Pentraxin-3 (*Ptx3*) is an acute-phase protein that regulates the immune system, including the complement system [81,82].

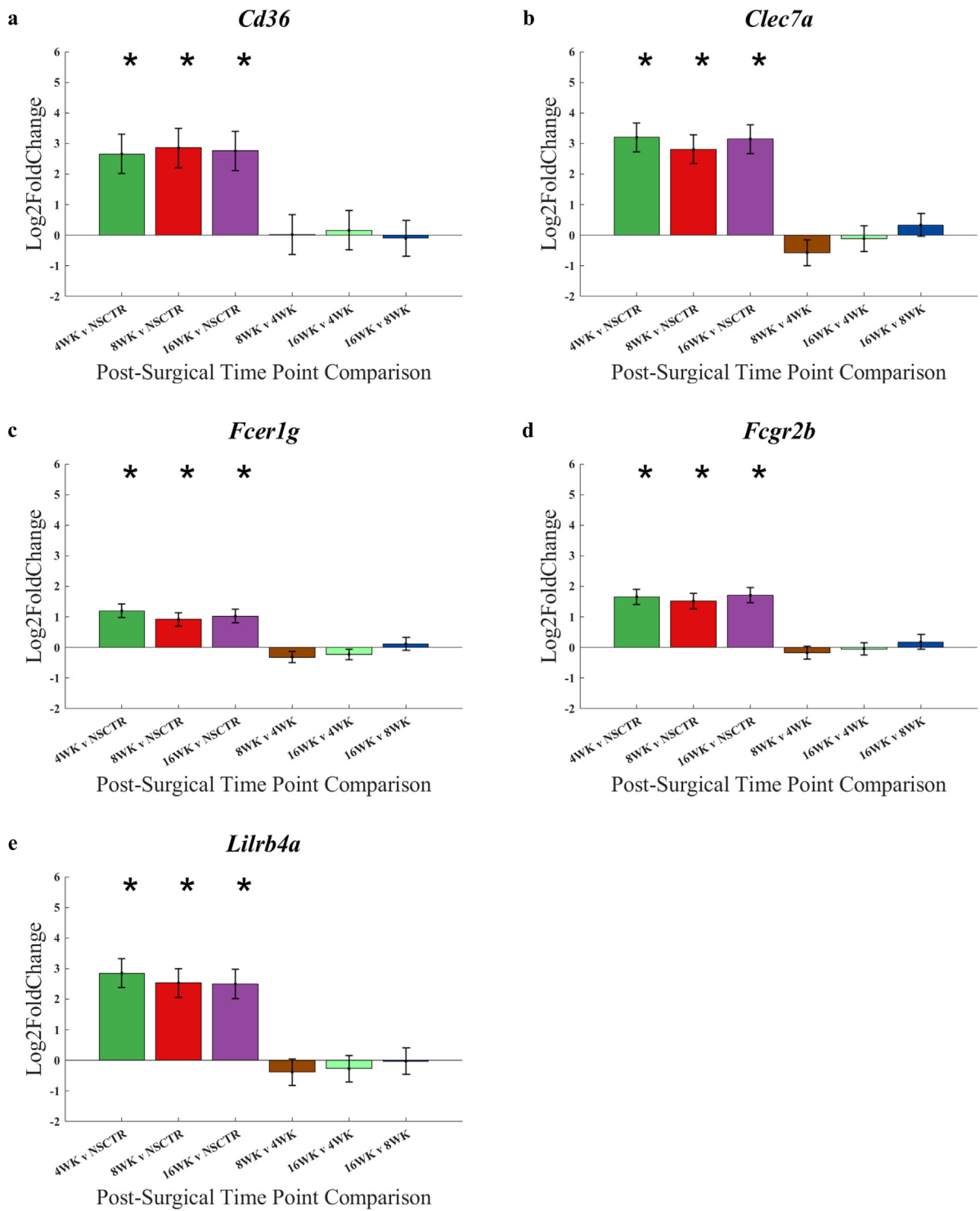
In addition to its role in innate immunity against various pathogens, the complement system is also responsible for foreign body response against biomaterials [83–85]. The complement cascade is activated by the adsorbed IgG or C3 directly on the biomaterial surface, which occurs immediately after biomaterial implantation. The adsorption leads to the activation of cellular responders and the production of pro-inflammatory cytokines and chemokines, activating an immune response against microelectrodes [86–88]. To date, we are unaware of any report directly linking the complement system's role and the failure of intracortical microelectrodes. However, the upregulation of complement factors suggests its role in tissue response against microelectrodes. The sustained upregulation of members of the complement system indicates that this process still occurs at chronic time points and may contribute to tissue response against microelectrodes at both acute and chronic time points.

## 5.2. Extracellular matrix

Matrix Metalloproteinases 12 (*Mmp12*) is a Matrix Metalloproteinase (MMPs) family member. MMPs are zinc-containing en-

dopeptidases that participate in the remodeling of extracellular matrix by breaking down extracellular matrix into its components [89]. In a previous study by Rennaker *et al.*, rats administered with Minocycline showed improved neural recording performances [46]. Minocycline is an antibiotic and a broad-spectrum immune modulator. Minocycline may reduce the neuroinflammatory response and limit post-surgical microbial infection, increasing microelectrode integration in the study. In addition, minocycline is a non-specific MMP inhibitor and may have also influenced extracellular matrix remodeling, providing an alternative pathway to microelectrode recording performance [90,91]. It is important to note that the mechanisms of action for Minocycline were not explored in detail in the initial Rennaker *et al.* manuscript or any follow-up studies.

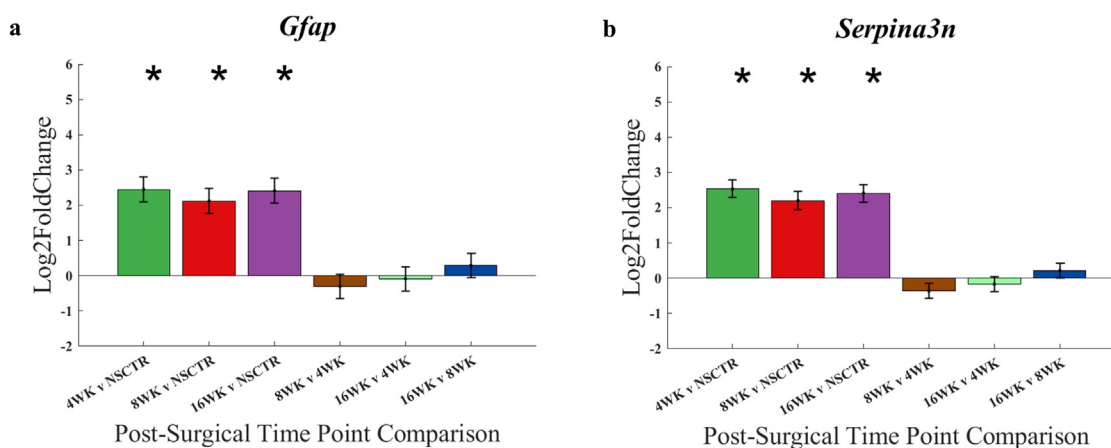
Secreted Phosphoprotein 1 (*Spp1*) is a part of the extracellular matrix of the central nervous system (CNS) and of the bone matrix, as well as a cytokine that regulates the immune response of the CNS [92]. In the CNS, macrophages express *SPP1*, which may activate microglia and contribute to neurodegeneration [92–94]. Cathepsin S (*Ctss*) is associated with extracellular matrix remodeling in the body, and its overexpression is associated with pulmonary fibrosis or aberrant extracellular matrix expression in the lungs [95]. Although the role of *Ctss* in extracellular matrix remodeling in the brain has not been extensively studied, *Ctss* is expressed by microglia in the central nervous system [96] and thus may play a role in glial scar formation around implanted intracortical microelectrodes.



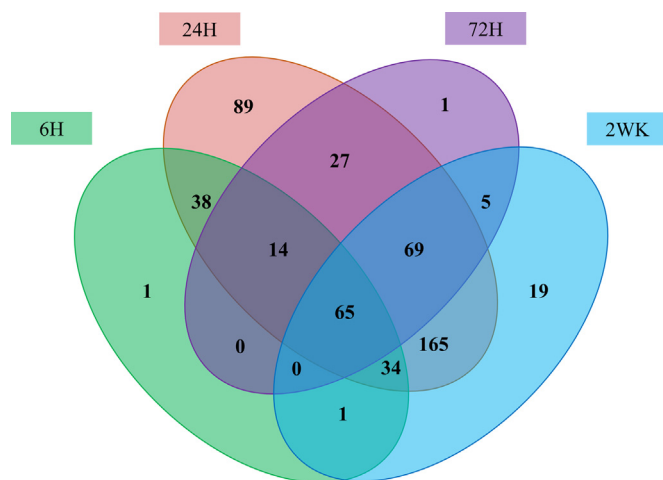
**Fig. 5.** Bar graph of differential gene expression of (a) *Cd36*, (b) *Clec7A*, (c) *Lilrb4a*, (d) *Fcgr1g*, and (e) *Fcgr2b* at 4WK vs. NSCTR (green), 8WK vs. NSCTR (red), 16WK vs. NSCTR (purple), 4WK vs. 8WK (brown), 4WK vs. 16WK (lime green), and 8WK vs. 16 WK (navy blue). The height of each bar shows the Log2FoldChange of comparison. The error bar indicates the standard error of the mean between gene expressions at each time point compared. Asterisk (\*) denotes  $P_{adj} < 0.05$ .

The extracellular matrix (ECM) in the central nervous system is unique compared to the rest of the body, consisting of minimal collagen and fibronectin, which are a significant component of the extracellular matrix for the rest of the body, and mainly comprised of proteoglycans, glycoproteins, linker proteins, and matricellular proteins [97,98]. Since ECM support allows for the communication between cells in the CNS, remodeling of the ECM may affect neuronal, microglial, astrocytic, and oligodendrocytic activity in the

tissue microelectrode interface, contributing to the chronic failure of microelectrode recording. Further, being that all three genes associated with the ECM that were detected to significantly change expression levels compared to NSCTR were consistently expressed at 4WK, 8WK, and 16WK post-surgery, our interpretation of the results is that the post-implantation ECM expression/composition is matured by 4WKs and remains stable throughout the remaining duration of microelectrode implantation. Therefore, changes in



**Fig. 6.** Bar graph of differential gene expression of (a) *Gfap* and (b) *Serpina3n* at 4WK vs. NSCTR (green), 8WK vs. NSCTR (red), and 16WK vs. NSCTR (purple), 4WK vs. 8WK (brown), 4WK vs 16WK (lime green), and 8WK vs 16 WK (navy blue). The height of each bar shows the Log2FoldChange of comparison. The error bar indicates the standard error of the mean between gene expressions at each time point compared. Asterisk (\*) denotes  $P_{adj} < 0.05$ .



**Fig. 7.** Gene expression at the microelectrode-tissue interface in acute time points. a) Venn Diagram indicating the number of genes differentially expressed for each time point examined, compared to the NSCTR mice at acute time points, based on data from a previously published study [63]. Overlapping regions of the Venn diagrams were used to show an overlap of differentially expressed genes at 4WK, 8WK, and 16WK post-surgery compared to naïve sham control mice,  $P_{adj} < 0.05$  and  $\text{Log2FoldChange} > 1$  or  $< -1$ .

recording performance between 4WK to 16WK post-surgery are likely not a result of changes in the extracellular matrix composition alone. However, immunohistology images of ECM proteins adjacent to microelectrode arrays have shown changes in the distribution of ECM components with time [65,99–103].

### 5.3. Cellular receptors

Cluster of Differentiation 36 (Cd36) is a glycoprotein expressed on the surface of platelets and macrophages. Cd36 is a scavenger receptor that recognizes thrombospondin, collagen, phospholipids, as well as oxidized LDL; and is a coreceptor for TLR4:TLR6 complex [104–106], leading to activation of macrophages via intracellular signaling pathway. Further, Cd36 also functions as an adhesion molecule [106,107]. C-Type Lectin Domain Family 7 Member A (Clec7a) is a glycoprotein on the surface of macrophages and B-lymphocytes with a C-lectin-like extracellular domain. Clec7a is a pattern recognition receptor that detects fungi and can lead to the activation of immune cells, as well as a co-stimulator of T-cells promoting T-cell activation [108–110]. Leukocyte Immunoglobulin-

like receptor Superfamily B member 4 (Lilr4a) is a glycoprotein expressed on macrophages and recognized MHC I expressed on antigen-presenting cells (APCs) [111]. Lilr4a downregulates the activation of macrophages and downregulates immune activity [111,112]. *Fcgr1g* encodes for a receptor for the Fc segment of IgE, while *Fcgr2b* encodes for a receptor for the Fc segment of IgG. *Fcgr1g* and *Fcgr2b* are expressed in astrocytes and microglia to facilitate the inflammatory response to immunoglobulins [113]. While the specific activities of each of these five genes are varied, the upregulation of them together likely reflects a well-coordinated and highly specified cell-mediated inflammatory response triggering further immune cell activation to chronic microelectrode implants. Receptor-ligand interactions have been a target of the biomaterials host response field for decades [114] and, more specifically, approached by those seeking to inhibit microelectrode-induced tissue responses [115,116]. The receptors indicated here could represent future targets to mitigate cellular responses to events following microelectrode implantation to improve chronic recording performance.

### 5.4. Other highly differentially expressed genes

Increased expression of glial fibrillary acidic protein (GFAP) is a marker for reactive astrocytosis or glial scar formation and a well-established marker for neuroinflammatory tissue response in the context of microelectrode implantation [31,32,71,117] – hence it was one of the custom-added genes to our custom assay set. *Gfap* gene expression is therefore congruent with our understanding of tissue response to intracortical microelectrodes that GFAP protein is stably upregulated at 4WK to 16WK time points post-implantation. *Serpina3n* encodes for the protein serine peptidase inhibitor clade A member 3n, and it is orthologous to  $\alpha 1$ -antichymotrypsin in humans. *Serpina3n* inhibits the proteolytic activity of Cathepsin G, leukocyte elastase, granzyme B, and matrix metalloproteinase 9 [118]. *Serpina3n* is often expressed in neurons and astrocytes after injury [119] and is overexpressed in mouse models of Alzheimer's and prion disease [120]. There are conflicting reports on the role of *Serpina3n* in neuroinflammation. Multiple studies have found *Serpina3n* to be neuroprotective: higher *Serpina3n* expression is associated with attenuating neuropathic pain, reducing the severity of Multiple Sclerosis, and reducing tissue damage in ischemic stroke [121]. Thus, higher expression of *Serpina3n* at chronic time points reported here may represent the upregulation of neuroprotective molecules after the initial neuroinflammatory response of the acute phase has begun to subside.

However, in one study of mice treated with neurotoxin, the neuroprotective effect of melatonin was lost when associated with *Serpina3n* overexpression [122]. Therefore, a controlled study intentionally overexpressing or inhibiting *Serpina3n* expression in an intracortical microelectrode implant model may resolve conflicting results.

### 5.5. Considering gene expression acute time points

While differential gene expression at chronic time points following microelectrode implantation is relatively stable, the differential gene expression at acute time points is more dynamic. The acute response has more upregulated genes, based on a related study using the same methods and also analyzed with nCounter technologies [63]. Of the 791 genes we investigated in the previous study (Note: in our current study, we used 826 genes as we expanded our panel) at 6H, 24H, 72H, and 2WK post-surgery, 65 genes were upregulated at all time points. There are 1, 89, 1, and 19 genes that are differentially expressed at only one of the time points, 6H, 24H, 72H, and 2WK post-surgery, respectively.

## 6. Conclusions

In this study, we investigated the expression of 826 genes in the neuroinflammatory pathway at the microelectrode-tissue interface in WT mice to investigate the differential expression of genes at chronic time points (4WK, 8WK, and 16WK) post-surgery. We aimed to identify persistently or increasingly differentially expressed genes that may hinder microelectrode integration or offer protective healing to the brain to improve the chronic recording performance of implanted intracortical microelectrodes.

We have found that the gene expression in the neuroinflammatory pathway post-surgery is stable between 4WK to 16WK post-surgery. Overall, 26 out of the 826 genes were identified to be upregulated and only 2 to be downregulated at any point in the study. Of the 28 differentially expressed genes, 68% (19) showed upregulation at all three time points investigated in this study. The stability of gene expression over time points considered to be more chronic found in this study is in contrast with previous studies at acute time points (using the same experimental methods) [63,68], which showed a dynamic upregulation of genes, peaking at 24–72 hours post-surgery. The highest upregulated genes identified in this study are *C3*, *C4a*, *Cd36*, *Cle7a*, *Gfap*, *Lilrb4*, *Mmp12*, *Serpina3n*, and *Spp1*. *C3* is a significant component of the complement system and was just one of four genes from the complement system that we found to be differentially expressed in this study. Therefore, *C3*, and more broadly, the complement system, may be strong candidates for therapeutic or gene inhibition studies to improve the integration of intracortical microelectrode and, eventually, their chronic recording performance. While three genes associated with the extracellular matrix were differentially expressed in this study, methods to manipulate extracellular matrix composition to facilitate microelectrode performance are more complex. However, five genes associated with cell surface receptors were differentially expressed in this study. The facilitation of cell-material interactions through various approaches has been shown to mitigate adherent cell density, morphology, proliferation, and function. It has been a popular strategy of the biomaterials community to improve biocompatibility for decades [123–127]. Therefore, the receptor pathways identified here also represent a target of interest for various approaches to mitigate their expression or ability to participate in the neuroinflammatory response to intracortical microelectrode implantation. Moving forward, the genes identified here in either the complement cascade or to be involved in receptor-mediated neuroinflammatory processes will be among the first we continue to explore.

One limitation of our research is that we inserted nonfunctioning probes in the brain to approximate tissue reaction to recording microelectrodes. While we can study the changes in gene expression at the microelectrode-tissue interface, we cannot directly correlate the tissue response to recording signal quality. Future studies using functioning microelectrodes will be able to better correlate the relationship between gene expression and the recording performance of intracortical microelectrodes. Another limitation is that the bulk analysis using tissue extracted manually by biopsy punch is less accurate than that of laser microdissection or spatial proteomics. While we visually check every tissue biopsied to ensure that the site of the implant is as close to the center as possible, even slight imprecision in the centering of the implantation site would lead to the measurement of gene expression beyond a 500  $\mu\text{m}$  radius of implantation site that may dilute the changes in gene expression at the implantation site and alter our results. Furthermore, even when the implantation site is located accurately in the biopsy center, the tissue further away from the implantation site is represented more due to a larger surface area, diluting the difference in gene expression within the tissue closer to implantation. One benefit is that the increased tissue leads to higher coverage of genes expressed; lower expressing genes are not easily missed. In addition, genes identified as differentially expressed using this method would likely exhibit even more differential expression closer to the implantation site.

Finally, it is essential to discuss that the current study could have been more extensive in spatial resolution and cell-specificity of gene expression. The study is also limited to gene expression. We are following up on this study with an in-depth investigation of the cell-specific and spatially resolved analysis of neuroinflammatory pathways with proteomic panels to complement the current research.

No matter the specific tools used, investigating gene expression at the microelectrode-tissue interface is valuable for studying the molecular process in response to microelectrode implantation for BMI applications. This tool should be applied in future studies of tissue response to different microelectrodes, comparing the effects of materials, size, shape, and flexibility on the gene expression and correlating with recording performance.

## Author contributions

JRC contributed to the conception and design of the work. SS contributed to the methodology, software analysis, validation, formal analysis, investigation, and data curation. ERC guided the statistical analysis of the work. LD assisted in the validation of the analysis. SS wrote the original draft and figures preparation as well as the review and editing along with JRC. JRC provided the funding and resources to conduct the study.

## Disclosures

The contents do not represent the views of the U.S. Department of Veterans Affairs, the National Institutes of Health, or the United States Government.

## Declaration of Competing Interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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